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Auteurs: Sampada Bodkhe, Gabrielle Turcot, Frederick Gosselin, & Daniel
Authors: Therriault

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One-Step Solvent Evaporation-Assisted 3D Printing of Piezoelectric PVDF Nanocomposite Structures

*Sampada Bodkhe, Gabrielle Turcot, Frederick P. Gosselin And Daniel Therriault**

AUTHOR ADDRESS

Laboratory for Multiscale Mechanics, Department of Mechanical Engineering,
Centre for Applied Research on Polymers and Composites (CREPEC)
Polytechnique Montreal,
C.P. 6079, succ. Centre-Ville, Montreal, QC H3C 3A7, Canada

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ABSTRACT

The development of a 3D printable material system, possessing inherent piezoelectric properties, to fabricate integrable sensors in a single-step printing process without poling is of importance to the creation of a wide variety of smart structures. Here, we study the effect of addition of barium titanate nanoparticles in nucleating piezoelectric β -polymorph in 3D printable polyvinylidene fluoride (PVDF) and fabrication of the layer-by-layer and self-supporting piezoelectric structures at micro to millimeter scale by solvent evaporation-assisted 3D printing at room temperature.

The nanocomposite formulation, obtained after a comprehensive investigation of composition and processing techniques, possesses a piezoelectric coefficient, d_{31} , of 18 pC N⁻¹ which is comparable to typical poled and stretched commercial PVDF film sensors. A 3D contact sensor that generates up to 4 V upon gentle finger taps demonstrates the efficacy of the fabrication technique. Our one-step 3D printing of piezoelectric nanocomposites can form ready-to-use complex-shaped, flexible and lightweight piezoelectric devices. When combined with other 3D printable materials, they could serve as stand-alone or embedded sensors in aerospace, biomedicine and robotic applications.

INTRODUCTION

Polyvinylidene fluoride (PVDF) is the most piezoelectric polymer. Although PVDF's piezoelectric properties are lower than ceramics, it scores over them in terms of the inherent advantages of biocompatibility, toughness, flexibility, formability and higher fatigue life.¹ Among the various crystalline phases of PVDF, the electroactive β -phase (all trans) with a planar zig-zag form,² imparts the highest dipole moment resulting in higher piezoelectric and ferroelectric constants. Unfortunately, PVDF commonly crystallizes into the thermodynamically stable non-polar α -phase upon solidification that does not possess the desired piezoelectric properties. The attainment of β -phase thus requires either one or more physical transformations via application of heat (annealing),³ large mechanical strain (stretching),⁴⁻⁶ large electric fields (poling),⁷⁻⁸ or filler addition.⁹⁻¹⁰ Fillers like carbon nanotubes,¹¹⁻¹² clay,¹³ cellulose,¹⁰ magnetic¹⁴ and piezoelectric nanoparticles (NPs)¹⁵ have proven to be very efficient in preventing the reversion of β -phase to α -phase upon solidification. The addition of eco-friendly and biocompatible¹⁶⁻¹⁷ piezoelectric ceramic filler - barium-titanate (BaTiO₃ NPs)¹⁸⁻²² into PVDF has also shown to improve the ferro and piezoelectric properties of PVDF without compromising on

its flexibility or strength. The incorporation of BaTiO₃ NPs into PVDF has been attempted so far via sonication^{21, 23-24} and ball-milling²⁵⁻²⁶ approaches.

Commercially available piezoelectric sensors essentially possess flat or fiber-like configurations and hence are limited to the use of single piezoelectric coefficient only for electromechanical coupling. Three-dimensional (3D) printing of piezoelectric materials benefits from improved electromechanical response extractable from 3D designs. Such an improvement stems from the synergistic augmentation of both accessible strain and coupling between both the in-plane and out-of-plane piezoelectric coefficients, thereby, increasing the voltage output and consequently, the sensitivity of the device.²⁷

For a piezoelectric sensor to be efficient, it will have to be integrated into the end-component. A multi-material 3D printing process can result in elimination of the additional manufacturing step of sensor-attachment, thereby, serving as a long-term solution. In all the previously developed techniques for 3D printing of piezoelectric polymers such as fused deposition modelling of PVDF,²⁸ optical printing of barium titanate (BaTiO₃) in a photoliable polymer,²⁹ near-field electrospinning of PVDF,^{30, 31} poling still dominates as an obligatory treatment. Further, the requirement of poling can be envisaged as a hindrance to achieve simultaneous integration of piezoelectric sensors during a multi-material 3D printing process. The concern is aggravated when the adjacent material or substrate properties are adversely affected by the poling conditions (e.g., degradation or melting of the polymer structure). Therefore, the removal of the poling step will not only simplify the printing process but at the same time allow: (i) multi-material printing; (ii) conformal printing on sensitive materials or systems; (iii) new opportunities for creating piezoelectric structures with complex configurations.

In this work, we engineered a nanocomposite formulation to attain a combination of printability and piezoelectric properties close to that of commercial PVDF films without the requirement of poling. To achieve the nanocomposite formulation, we compared three different methods: ball-milling, extrusion mixing, and sonication to incorporate varying concentrations of BaTiO₃ NPs in PVDF. The ability of the nanoparticles to nucleate and further retain the β -phase in PVDF is studied through custom designed piezoelectric tests and available characterization techniques: scanning electron microscopy (SEM), X-ray diffractometry (XRD), fourier transform infra-red photo-acoustic spectroscopy (FTIR-PAS) and impedance spectroscopy. The formulation showing the best piezoelectric properties is then utilized to form micro to millimeter scale 3D features via solvent evaporation-assisted 3D printing. The process involves the dissolution of the nanocomposite into a highly volatile solvent followed by extrusion through a small nozzle under applied pressure.³²⁻³³ The rapid evaporation of the solvent results in retention of the desired shapes: layer-by-layer, self-supporting and even freestanding structures.³² The application of our work is highlighted in the form of a ready-to-use millimeter scale 3D contact sensor fabricated in a single printing step.

EXPERIMENTAL SECTION

Methods

A mixture of acetone (BDH) and dimethyl formamide (DMF; Alfa Aesar) was chosen as the solvent system for polyvinylidene fluoride (PVDF; Sigma Aldrich). DMF is considered the least hazardous among the solvents used for PVDF and has a boiling point of about 153 °C.³⁴ On the other hand, acetone has a low boiling point (~56 °C) but cannot dissolve PVDF. The ratio of DMF: acetone was experimentally optimized to 40:60 to minimize the amount of DMF, while facilitating a quicker shape retention during printing. Dimethyl sulfoxide (DMSO; Sigma

Aldrich; 65 g L⁻¹) was added as a β -phase initiating agent.³⁵ PVDF (2 g) was sonicated with DMF (4 mL), acetone (6 mL) and DMSO (0.6 mL) for 20 min to form a 0.2 g mL⁻¹ solution for printing. A similar solution was also used to fabricate a solution cast film for comparison.

Barium titanate nanocomposite preparation (0.2 g mL⁻¹ nanocomposite in the solvent mixture)

Ball-mill mixing: A mixture of Barium titanate NPs (BaTiO₃; 99.9% purity, 100 nm; Nanostructured & Amorphous materials Inc.; 0.2 g) and PVDF (2 g) was sonicated in DMF for 2 h. The solution was then mixed in a high energy shaker ball-mill (SPEX SamplePrep™ 8000 Series Mixer/Mill™) at a rate of 1080 cycles per minute for 20 minutes. The number of zirconia balls for milling was chosen to match the weight of the solution. The solution was dried in a vacuum oven at 60 °C for 12 h to remove all the DMF. The dry nanocomposite (2 g) was later sonicated with DMF (4 mL), acetone (6 mL) and DMSO (0.6 mL) until complete dissolution of the nanocomposite was achieved. For apparent viscosity tests and printing 3D structures, 2.5 g and 3.0 g of the nanocomposite were dissolved to form 0.25 and 0.3 g mL⁻¹ solutions, respectively.

Extrusion mixing: A mixture of BaTiO₃ NPs (0.2 g) and PVDF (2 g) was fed into a 5 mL twin screw micro extruder (Xplore®) at 185 °C and mixed for 5 minutes. A temperature of 185 °C was maintained above the melting point of PVDF ($T_m = 171$ °C)³⁶ at both the inlet and exit of the extruder. The screw speed was 200 rpm. The mixture of PVDF and the NPs (2 g) obtained in the form of the filaments from the extruder was sonicated with a mixture of DMF (4 mL), acetone (6 mL) and DMSO (0.6 mL) until complete dissolution of the nanocomposite was achieved.

Sonication: BaTiO₃ NPs (0.18 g) were added to DMF (4 mL) and sonicated for 3 h to achieve complete dispersion. PVDF (1.8 g) was completely dispersed separately in acetone (6 mL) via sonication. The two solutions were mixed and DMSO (0.6 mL) was added and sonicated for 20 minutes.

Solvent evaporation-assisted 3D printing

PVDF and its nanocomposite solutions were poured into a syringe (3 mL) and placed into a pneumatically operated dispensing system (HP-7X, EFD) to apply precise pressures for printing, as depicted in Figure 1a. This dispensing system was mounted on a robotic head (I&J2200-4, I&J Fisnar Inc.) controlled by a commercial software (JR Points for Dispensing, Janome Sewing Machine) that further enabled the deposition of the inks on a movable stage. The geometry of the profile to be printed was communicated to the robotic arm as a series of coordinates through the software. The air pressure from the dispenser forced the material out of the syringe through a nozzle. As the material escaped the nozzle, the evaporation of the solvents provides rigidity to retain the designed geometry. To fabricate one-dimensional (1D) filaments, two-dimensional (2D) films and, and 3D layer-by-layer and self-supporting structures, different solution concentrations (0.2, 0.25, and 0.3 g mL⁻¹) were used with a metallic nozzle (inner diameter = 100 μm) and varying extrusion pressures, P (0.1 to 2 MPa) and robot speeds (0.5 – 20 mm s⁻¹). While fabricating films, the concentration of nanocomposite in the solvent mixture was kept at 0.2 g mL⁻¹ and the printing parameters were: nozzle inner diameter = 100 μm; $P \sim 1$ MPa; robot speed = 20 mm s⁻¹, unless mentioned otherwise.

Characterization

To fabricate the sensors a thin conductive electrode layer was painted on both sides of the printed nanocomposite films and the internal and external surfaces of the 3D cylinder with commercially available conductive silver paste (Sigma Aldrich). Electrical connections were made using a conducting aluminum tape (3M).

To determine the linearity of the sensors a dynamic mechanical analyzer (DMA; Q800; TA instruments) was further used in a single frequency (45 Hz) tension mode with a multi-stress force ramp of 0.1 N until fracture (rate of 0.5 N min⁻¹). The sensors consisting of films (20 mm × 5 mm × 0.1 mm) with electrodes (10 mm × 5 mm) were used with a grip separation of ~ 10 mm. Three samples were tested for each concentration: 5, 10 and 15 wt.% of NPs in the nanocomposites. Piezoelectric charges obtained from all the sensors were converted into voltages using a charge amplifier (Piezo lab amplifier, MEAS specialties) in charge mode; acquired with a data acquisition system: NI-9239, attached to a USB carrier NI-9162 (National Instruments) and recorded using a LabVIEW interface.

To obtain the diffractogram patterns of the films a Philips X'pert diffractometer was used with scan angles from 10° to 50°. A scan rate of 0.4 ° min⁻¹ was used with a Cu target and K_α radiation at 50 kV and 40 mA. Fourier transform infrared (FTIR) – Photo acoustic spectroscopy (FTS 6000 spectrometer, Bio-rad) was used to obtain the absorption spectra of PVDF and its nanocomposite films in the range of 500 – 4000 cm⁻¹. 128 scans were conducted on each sample with a resolution value of 8 cm⁻¹.

For viscosity characterization five identical filaments were printed (nozzle diameter = 100 μm; speed = 0.5 mm s⁻¹; printing time = 120 s) at different pressures (0.1 – 2 MPa) using 0.20, 0.25, and 0.30 g mL⁻¹ of ball-milled PVDF/ BaTiO₃ nanocomposite in the solvent mixture. End effects

were neglected as the length to diameter (L/D) ratio of the nozzle was greater than 50.³⁷ The weights of the filaments were determined after 48 h to ensure complete evaporation of solvents. Mass flow-rates were calculated by reverting to the original mass before solvent evaporation. The apparent viscosity calculation details are provided in the supporting information and in Bruneaux *et al.*³⁸

To image structures printed with the nanocomposites optical microscopy (BX-61 Olympus microscope; Image-Pro plus V5, an image processing software from Media Cybernetics) was used. The morphology and cross-sections of the 3D printed films and structures were observed using a field emission scanning electron microscope (FE-SEM; JEOL JSM-7600TFE). An SEM (JEOL JSM 840) was used to obtain the images of the 3D printed structures at lower magnifications. Both SEM were operated at an accelerating voltage of 10 kV. For viewing the cross-sections, the fibers and films were fractured in liquid nitrogen. All the structures and films were gold coated before imaging.

RESULTS AND DISCUSSION

Figure 1a schematizes the one-step solvent evaporation-assisted 3D printing of a piezoelectric nanocomposite contact sensor. The 70-layer cylindrical sensor shown in Figure 1b was printed with 0.25 g mL^{-1} of 10 wt.% BaTiO₃ NP ball-milled nanocomposite solution. The programmed diameter and height of the cylinder were 5 and 7 mm, respectively. After solvent evaporation, the printed cylinder shrunk to ~ 3.1 mm in both height and outer diameter. The 3D contact sensor was used right after printing, without the need for a poling step. The sensor was gently tapped with a forefinger (Figure 1b) consecutively, five times, and the generated signal can be seen in Figure 1c. The sensor produced a consistent maximum voltage output of ~ 4 V for touching and ~ -2 V upon releasing (see Figure S7 for the detailed mechanism). The 3D sensor produced

approximately ten times higher voltage than a film sensor of the same electrode surface area (Figure S6). The high voltage outputs from the 3D sensor presented here result from the improved inherent piezoelectric properties of PVDF by extrusion based printing and the addition of BaTiO₃ NPs. The contribution from interfacial charges to the response of the 3D sensor can be neglected as both the filler and the polymer used in this case are dielectrics,³⁹ and nanoscale particles have a negligible contribution towards Maxwell-Wagner effects.⁴⁰ Literature also suggests that addition of pristine BaTiO₃ nanoparticles to PVDF does not result in interfacial polarization.⁴¹

In the following paragraphs, the effect of four parameters on the piezoelectric properties of PVDF is investigated: (i) extrusion based printing; (ii) filler addition; (iii) processing techniques; and finally (iv) filler concentration. We use XRD and FTIR-PAS to study the effect of solvent evaporation-assisted 3D printing of PVDF on the conversion of its α -phase into β -phase.⁴² The XRD patterns of solution-cast and 3D printed PVDF films prepared by using 0.20 g mL⁻¹ PVDF in the solvent mixture can be observed in Figure 2a. Peaks pertaining to the α -phase of PVDF at 18.70°, 20.04° and 26.50° are clearly visible in case of the film fabricated via solution casting route,^{13, 43} whereas a single distinct peak at 20.26° corresponding to the β -phase confirms the effect of the extrusion pressures in the attainment of β -phase. As the polymer chains come out of the nozzle, the extrusion pressure of ~1 MPa leads to the significant phase transformation and the passage through the relatively long slender nozzle (12.7 mm; L/D ratio = 127;) can align the polymer chains. We then carried out FTIR on the two kinds of films discussed above. Bands at 763 and 974 cm⁻¹ are known to represent the presence of α -phase and those at 512, 840 and 1279 cm⁻¹ that of β -phase in PVDF.⁴⁴⁻⁴⁶ As seen from a large drop in absorbance at ~763 cm⁻¹ in Figure 2b, the fraction of β -phase, $F(\beta)$, considerably increased upon 3D printing. The $F(\beta)$, calculated

using Beer Lambert's law (Equation S2), in the 3D printed film (64%) was found to be ~30 % higher than the solution-cast film (49%).

To further improve the $F(\beta)$ in PVDF, we incorporated 10 wt.% BaTiO₃ NPs into the PVDF matrix. We compared three mixing methods—ball-milling, extrusion, and sonication—to determine which one had the most favorable impact on the piezoelectric voltage outputs resulting from the application of a dynamic mechanical load using the DMA. As the film based sensors were subjected to longitudinal loads (direction 1), charges were generated across the thickness (direction 3) of the film (Figure S2c). The maximum voltage output was obtained with the sensors fabricated from the ball-milled nanocomposites (Figure S3a). For these sensors, the peak-to-peak voltage saturated at 6 V for frequencies higher than 35 Hz. In comparison, the sensors fabricated by extrusion, and sonication failed to give outputs distinguishable from the noise. In addition, there was no voltage output from a sensor fabricated by ball-mill mixing of 10 wt.% BaTiO₃ NPs with polylactic acid (PLA), which ascertains the fact that this process works due to the enhancement of β -phase in PVDF and not due to the piezoelectric properties of the NPs. Additionally, BaTiO₃ is ferroelectric in nature and is rendered piezoelectric only upon electric poling. This strengthens the fact that the piezoelectric response obtained in our material is purely from PVDF and has no contribution from the nanoparticles.⁴⁷

We employed SEM and XRD characterization to understand why solely the ball-milled nanocomposites exhibited piezoelectricity. Figure 3a shows SEM image of BaTiO₃ NPs. The size of the NPs varies between 80-100 nm. The SEM images in Figure 3b-d show the morphology of the nanocomposites films. In the case of ball-milled nanocomposites (Figure 3b) large crystallites and pore sizes reveal higher crystal growth; a uniform dispersion of nanoparticle agglomerates (highlighted by circles) is also seen. It has been reported that

dispersed agglomerates of NPs lead to an increased space charge density which in turn leads to higher piezoelectric properties.⁴⁸ Non-uniformly distributed clusters are observed in the extruded nanocomposite (Figure 3c). There is more nucleation of crystallites in the sonicated nanocomposite (Figure 3d) as smaller spherulites are evident. Higher nucleation prohibits the growth of crystallites.⁹ The uniform dispersion of nanoparticles (seen as tiny white dots) in the sonicated nanocomposite is possibly the reason for this higher nucleation. Large micron-sized pores are present throughout the surface (Figure 3b) and cross-section (Figure S4) of the ball-milled nanocomposite films whereas internal pores are very small or absent in the extrusion-mixed and sonicated nanocomposites. The highly porous structure of ball-milled nanocomposites resulted in lower modulus as found by the mechanical tests (Figure S1b). Increased flexibility allows for soft sensor applications and reduced interference with sensed structures.

Figure 4a shows the X-ray diffractogram of the BaTiO₃ NPs with characteristic peaks of BaTiO₃ at 22.15°, 31.53°, 39° and 45°. ⁴⁹ The splitting of peaks belonging to the (200) and (002) planes at ~45° indicates the presence of tetragonal crystal structure, which is essential for spontaneous polarization and thus, piezoelectricity. ^{21, 47, 50} Figure 4b shows the X-ray diffractogram of PVDF nanocomposites prepared by ball-milling, extrusion, and sonication. In the nanocomposite prepared by the ball-milling approach, the peaks at 18.70°, 20.04° and 26.50° belonging to α -phase of PVDF are absent. ^{13, 43} The presence of a single broad peak at 2-theta value of 20.26° corresponding to the (200) and (110) planes^{13, 43} of β -phase underscores the inference that nanocomposite films prepared by ball-milling approach crystallized only in β -phase. In the case of the samples prepared by sonication, visible α -peaks are found at 18.7°. ^{13, 43} A prominent α -peak at 40° and a γ -peak close to 26° is seen in the extrusion-mixed sample. ⁵¹⁻⁵³ Uniformly dispersed individual nanoparticles in sonicated films were probably not as efficient as the

agglomerates present in the ball-milled nanocomposites in preventing the reversion to α -phase during the crystallization process. High temperature shear during extrusion shifted the BaTiO₃ tetragonal peak at 45°, depicting a change from the tetragonal structure of BaTiO₃ to a non-piezoelectric cubic structure.⁵⁴⁻⁵⁵ This may be linked to the temperature used for melt-mixing i.e., 185 °C which is higher than the BaTiO₃'s Curie temperature of 120 °C.⁵⁶ As there is a change from non-centrosymmetric to a symmetric crystal lattice, the melt-mixed nanocomposites could not exhibit piezoelectricity. The properties of BaTiO₃ NPs seem to be unaltered by the ball-milling process as no change in their peak locations is observed.

After determining that ball-milling is the most appropriate mixing method in terms of piezoelectric properties, three different nanoparticle loadings (5, 10 and 15 wt.%) were investigated to determine the optimum filler weight fraction to fabricate 3D sensors. The voltage responses from the single frequency scans observed in Figure 5 are linear with the force until fracture, as should be the case with piezoelectric materials. The voltage outputs initially increased from 5 wt.% of BaTiO₃ to 10 wt.%. However, the nanocomposite sensors with 15 wt.% of the fillers exhibited no considerable output. A maximum peak-to-peak voltage around 2.8 V was obtained at a force of 2.7 N for the sensor with 10 wt.% fillers.

Impedance spectroscopy was used to calculate the dielectric constants of the sensors. The nanocomposites with 10 wt.% NP loading possessed the highest dielectric constant of ~210 (Table S2). The piezoelectric coefficient is the ratio of electric field produced in a piezoelectric material to the applied stress. Average piezoelectric coefficients $d_{31} = 2.5$ and 18 pC N^{-1} were obtained for ball-milled nanocomposite sensors with 5 and 10 wt.% BaTiO₃ NPs, respectively (calculated using the voltage values as in Figure 5 and Equation S1). The value of 18 pC N^{-1} ,

obtained here without any poling, is comparable to that of typical commercial stretched and poled PVDF-based film sensors (23 pC N^{-1}).⁵⁷

We further use the results from SEM, XRD and FTIR to understand the performance of our ball-milled nanocomposites. Figure 6a-c are SEM images of 5, 10 and 15 wt.% of BaTiO₃ NPs in PVDF via ball-milling. Fewer number of agglomerates are found in the case of the 5 wt.% loading as compared to the 10 wt.%. Although the number of agglomerates is increased in the 15 wt.% loading, their average size is almost halved in comparison to the 10 wt.% loading. This establishes that there has to be an optimum size and number of agglomerates to effectively prevent the reversion to α -phase. The XRD results (Figure S5) depicted that the films prepared with 10 wt.% NP loading exhibited no other phases than β -phase while the other two films crystallized additionally in α or γ -phase or both.

FTIR-PAS was employed to explain the difference between the piezoelectric constants of the 5 and 10 wt.% nanocomposites. Figure 6d shows the FTIR spectra of the 5 and 10 wt.% ball-milled nanocomposite films. A clear decrease in the content of α -phase can be observed in the curve pertaining to 10 wt.% nanoparticle loading. Beer-Lambert's law was used to quantify this difference in the amount of the two phases in the nanocomposites. The $F(\beta)$ present in the 5 and 10 wt.% ball-milled nanocomposites was 68 and 78%, respectively (Equation S2). The higher value of $F(\beta)$ in the 10 wt.% nanocomposites explains the improved response and higher piezoelectric coefficient value. The Beer-Lambert law could not be applied to the 15 wt.% loaded nanocomposite (data not shown) due to the presence of additional γ -phase as seen from the XRD (Figure S5).

Piezoelectric fillers do not contribute to the overall piezoelectricity of the nanocomposite when used in very small quantities, which was the case until 10 wt.% loading.⁵⁸ Hence, the increased presence of β -phase in PVDF upon the addition of 10 wt.% NPs via ball-milling is attributed to the mechanical activation of the NPs and their dispersed agglomerates leading to an increased dipole moment.^{26, 48} Further, given that the piezoelectric coefficients of the filler and the polymer have different signs, poling in a single direction would cancel out the d_{31} coefficients.⁵⁹ Hence, our approach to orient dipoles without the application of any electric field serves to improve the inherent piezoelectric properties in PVDF at low mass fraction. Lower effective Young's modulus in the case of the ball-milled nanocomposites as compared to the other two nanocomposites, (Figure S1b) resulted in increased sensitivity.⁶⁰ However, as the process relies on improving the inherent piezoelectric properties of the polymer, factors such as humidity, temperature, print directions, speeds and pressures can have a strong effect on the properties and hence, reproducibility. Thus, efforts are being made to optimize these parameters and will form a part of our future work.

We propose the following hypothesis to summarize the process of formation of aligned β -phase chains during 3D printing. As seen in Figure 7, the addition of BaTiO₃ NPs to PVDF via ball-milling led to increased activation sites⁶¹⁻⁶² on the NPs acting as β -phase nucleating sites because of the strong O-H \cdots F-C hydrogen interaction at the PVDF/BaTiO₃ interfaces.⁶³ These interactions combined with the dipolar interactions of polar DMF and PVDF resulted in CH₂-CF₂ dipoles as in the case of all trans structure of β -phase. Moreover, the dipole alignment in our work is attained through mechanical means and not from conventional electrical poling.⁶⁴ The extensional flow of the solution resulted in the required chain and dipole alignment.⁶⁵⁻⁶⁶ Indeed the high pressures (\sim 1 MPa) during the passage through the fine nozzle with a high L/D

ratio (~120) and post-extrusion stretching due to higher velocities of the robotic motion (~20 mm s⁻¹) contributed to align the PVDF polymer chains. The sub-micron sized agglomerates further prevented any chances of reversion to α -phase.⁴⁰ In the absence of electric poling, the ferroelectric BaTiO₃ NPs could not contribute to the improved piezoelectricity.

The shape and thickness of the extruded material from the nozzle during the printing process predominantly depends on the relationship between the applied pressure and the relative velocity of the robotic-arm over the stage. Thus, to attain the required geometry, it is essential to arrive at the optimal relationship between the extrusion pressure and the velocity of the arm-movement via a rheological analysis.³³ Rheological characterization allows us to establish the dependence of apparent viscosity on the extrusion pressure and the printing speed. The former is proportional to the shear stress at the wall, whereas the latter relates to the shear rate during the printing process. Figure 8 shows the process-related viscosity as a function of the applied shear rates. The viscosity range for the three different concentrations: 0.2, 0.25 and 0.3 g mL⁻¹ of ball-milled PVDF/ BaTiO₃ nanocomposite, is found to be between 0.1 to 2.7 Pa s. The viscosity decreases with increasing shear rate, characteristic of a shear thinning behavior.⁶⁷ This property is essential for a material to be employed in extrusion-based printing processes. The optimal viscosity for a material is low enough to be extruded out of the small nozzle but at the same time high enough for shape retention after extrusion.⁶⁸ Thus, the rheological properties of the inks are well suited for 3D printing. Moreover, it can be observed that the viscosity of the inks significantly increases with the concentration of the nanocomposites in the solutions aiding the fabrication of 3D self-supporting structures due to the increased rigidity.

The viscosity study aided in determining the optimum concentrations of the ball-milled PVDF nanocomposite required to obtain 1D, 2D and 3D shapes as shown in Figure 9. We can see an

SEM image of the cross-section of a 1D filament (Figure 9a) extruded using 0.3 g mL^{-1} nanocomposite solution with a $100 \text{ }\mu\text{m}$ nozzle at $\sim 2.6 \text{ MPa}$. The average diameter of the fiber after complete evaporation of the solvents was about $56 \pm 6 \text{ }\mu\text{m}$. The reduction in diameter of the fiber and the rough surface upon extrusion is attributed to evaporation of the solvents post extrusion. A loading of 0.2 g mL^{-1} of nanocomposite in the solution-mixture was observed to be optimal for printing 2D films and patterns without voids or gaps. A 2D pattern: LM2 (Figure 9b; the abbreviation of our laboratory) was printed using 0.2 g mL^{-1} solution with a pressure of $\sim 0.11 \text{ MPa}$ and robot velocity of 10 mm s^{-1} . A concentration of 0.25 g mL^{-1} facilitated the formation of 2.5D layer-by-layer structures: a circular cylinder (Figure 9c) printed at $\sim 0.48 \text{ MPa}$ and 1 mm s^{-1} . The cylinder has 70 layers, and a programmed diameter and height of 5 and 7 mm, respectively. The concentration of 0.3 g mL^{-1} of the nanocomposite was best to print spanning or self-supported structures like 3D scaffolds. A 9-layer scaffold (Figure 9d) was printed at $\sim 1.3 \text{ MPa}$ and 13 mm s^{-1} using a $100 \text{ }\mu\text{m}$ nozzle with clearly distinguishable self-supporting filaments and individual layers. The spanning distance between two consecutive parallel filaments is 10 mm.

CONCLUSION

The fusion of the solvent evaporation-assisted 3D printing and our piezoelectric material results in two critical achievements: (i) genesis and stabilization of electroactive β -phase leading to remarkable sensing and actuation characteristics at room temperature, and (ii) optimized rheology to fabricate self-supporting structures with satisfactory mechanical robustness, all without the need for additional electromotive (poling) treatment. High dielectric and piezoelectric properties were obtained via 3D printing of a nanocomposite solution of 10 wt.% BaTiO_3 NPs ball-milled with PVDF due to the prevalence of β -phase. A piezoelectric coefficient of 18 pC N^{-1} comparable to that found in commercial PVDF sensors was obtained. A fully

functional 3D printed sensor generating a maximum voltage output of up to 4 V upon finger tapping was fabricated and demonstrated. The one-step 3D printing of piezoelectric materials opens up a new demographic of sensor designs that are more integrable, conformable, scalable, versatile, and application oriented. Apart from sensing, 3D piezoelectric scaffolds fabricated by the shown process could be used as electroactive scaffolds in tissue engineering⁶⁹ providing a biomimetic environment for cell culture. Given the limitation of the conventional electrode deposition (forming planar electrodes) techniques, there is a need to develop a hybrid process to print the electrodes along with the polymer, thereby, delivering the entire sensor in a single step. The sensors produced in the single step could be used as hair-like sensors for aerodynamics, as embedded sensors in aerospace or biomedical prosthesis and as filaments for smart textiles.

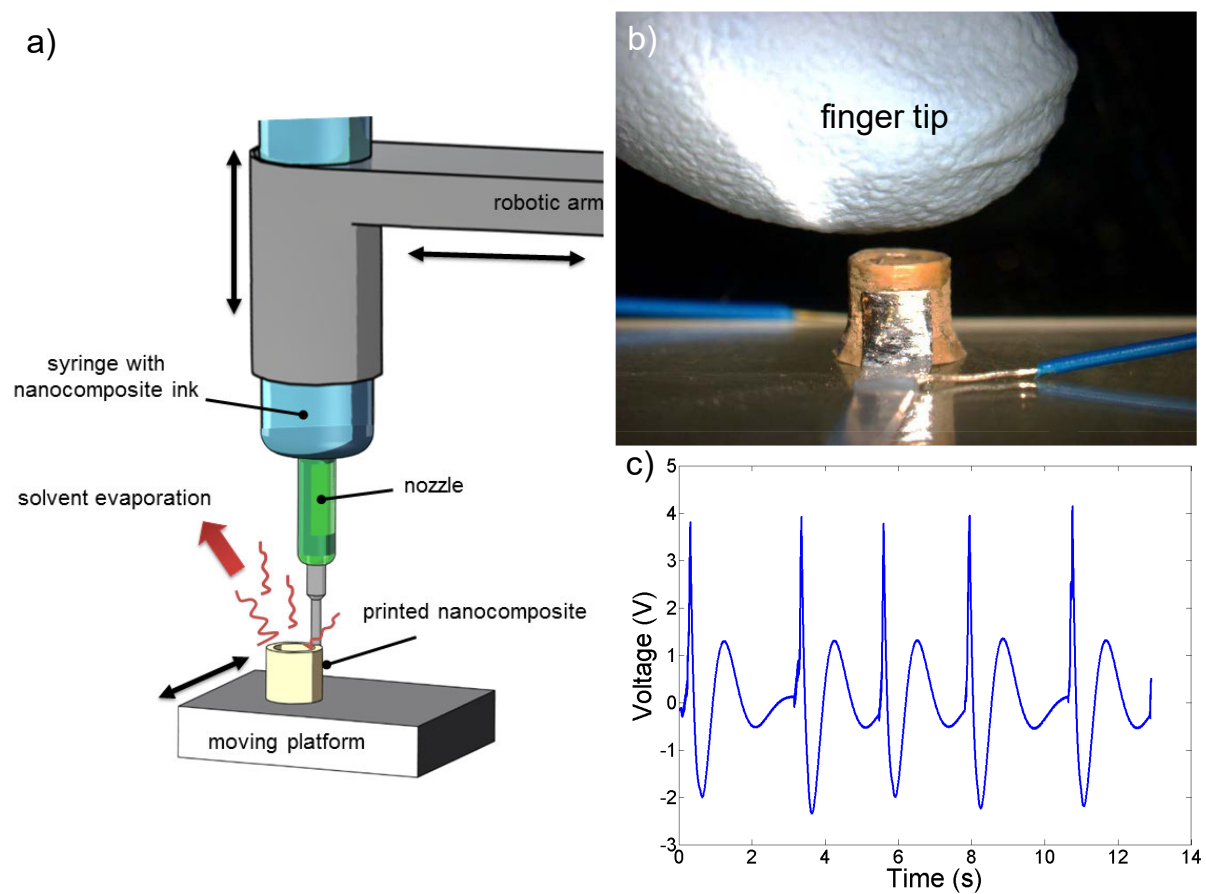


Figure 1. (a) Solvent evaporation-assisted 3D printing process for PVDF nanocomposite based 3D structures; (b) photograph of the 3D cylindrical sensor during a finger-tap test; (c) piezoelectric voltage output of the 3D cylindrical sensor upon five consecutive finger taps.

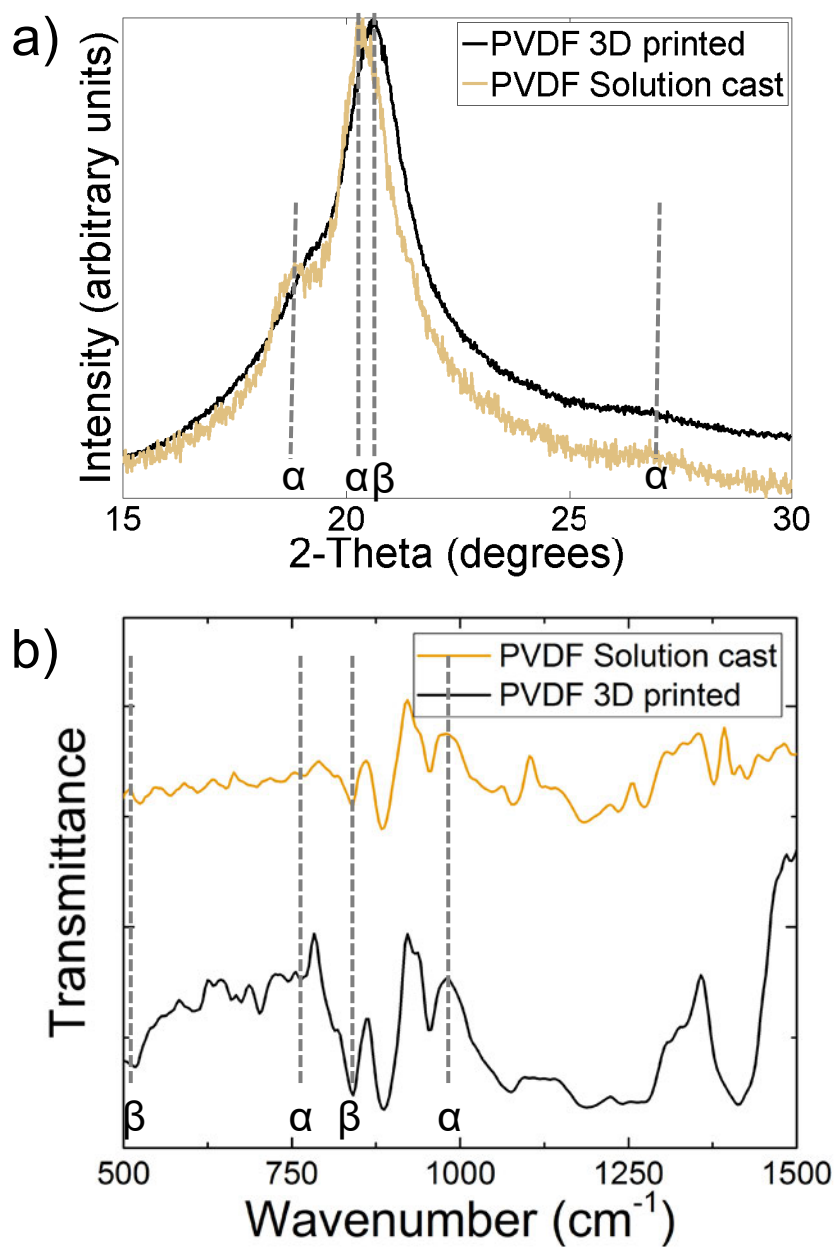


Figure 2. (a) X-ray diffractogram and (b) FTIR curves of 3D printed and solution-cast neat PVDF films (0.2 g mL^{-1} of PVDF in solvents). The characteristic peaks of the two phases of PVDF are labelled with their respective symbols ‘ α and β ’. (printing parameters: $\sim 1 \text{ MPa}$, 20 mm s^{-1} with a $100 \text{ }\mu\text{m}$ nozzle).

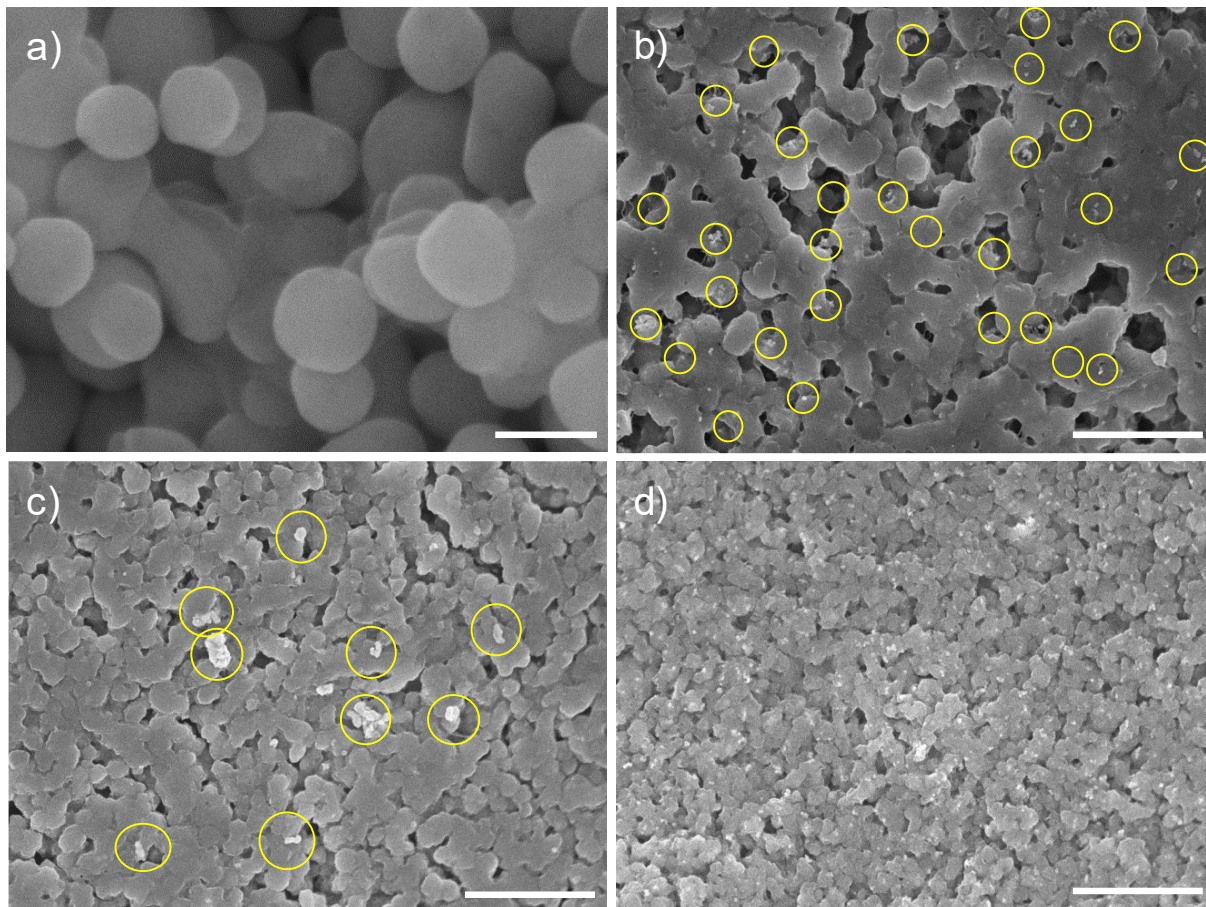


Figure 3. (a) SEM image of BaTiO₃ NPs (scale bar = 100 nm). SEM images of surfaces of films fabricated from the 0.2 g mL⁻¹ solutions of nanocomposites prepared by (b) ball-milling, (c) extrusion and (d) sonication (scale bars = 5 μm). Yellow circles highlight the BaTiO₃ NP agglomerates. (printing parameters: ~1 MPa, 20 mm s⁻¹ with a 100 μm nozzle)

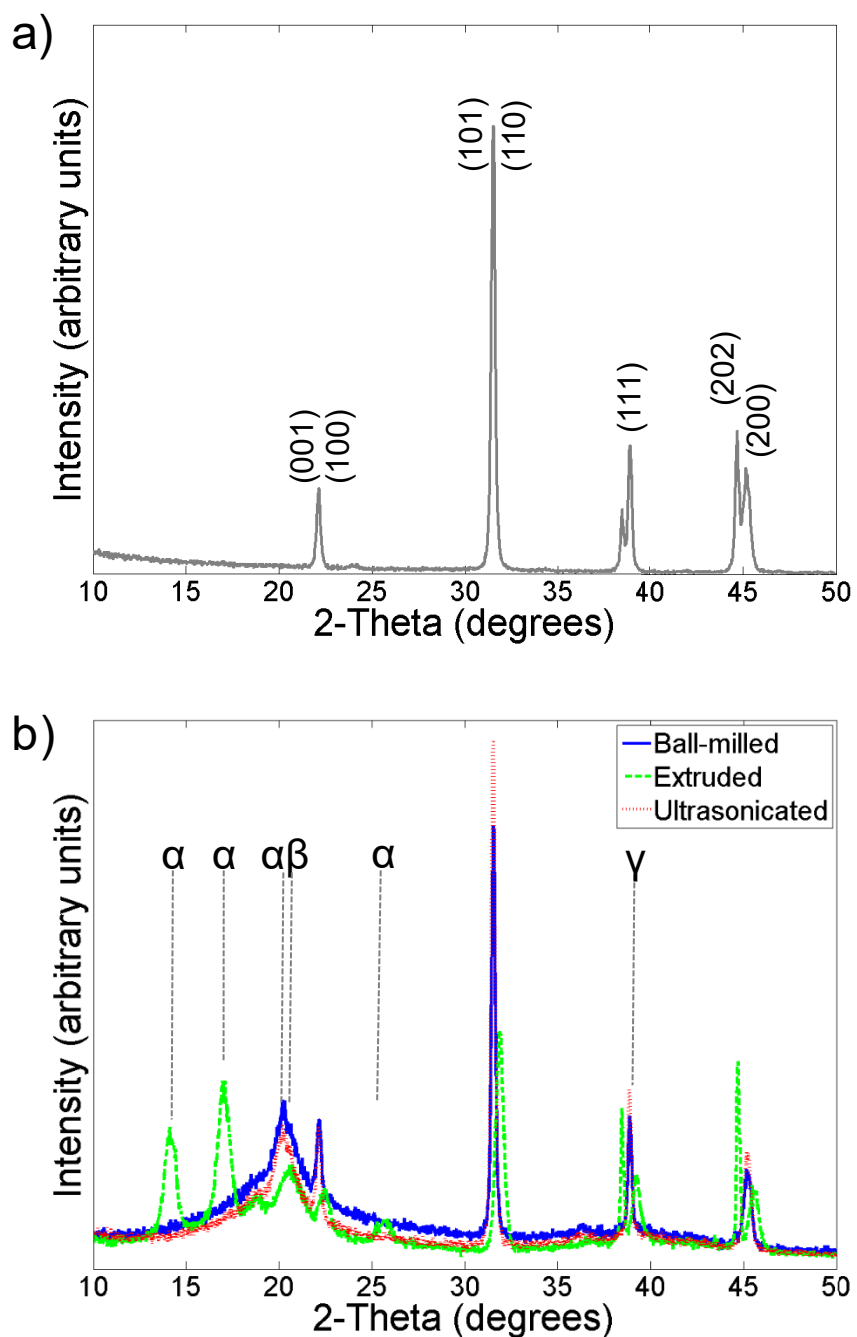


Figure 4. X-ray diffractogram of (a) BaTiO₃ NPs and (b) nanocomposites of 10 wt.% BaTiO₃ NPs and PVDF prepared by ball-milling, extrusion and sonication (printing parameters: ~1 MPa, 20 mm s⁻¹ with a 100 μm nozzle).

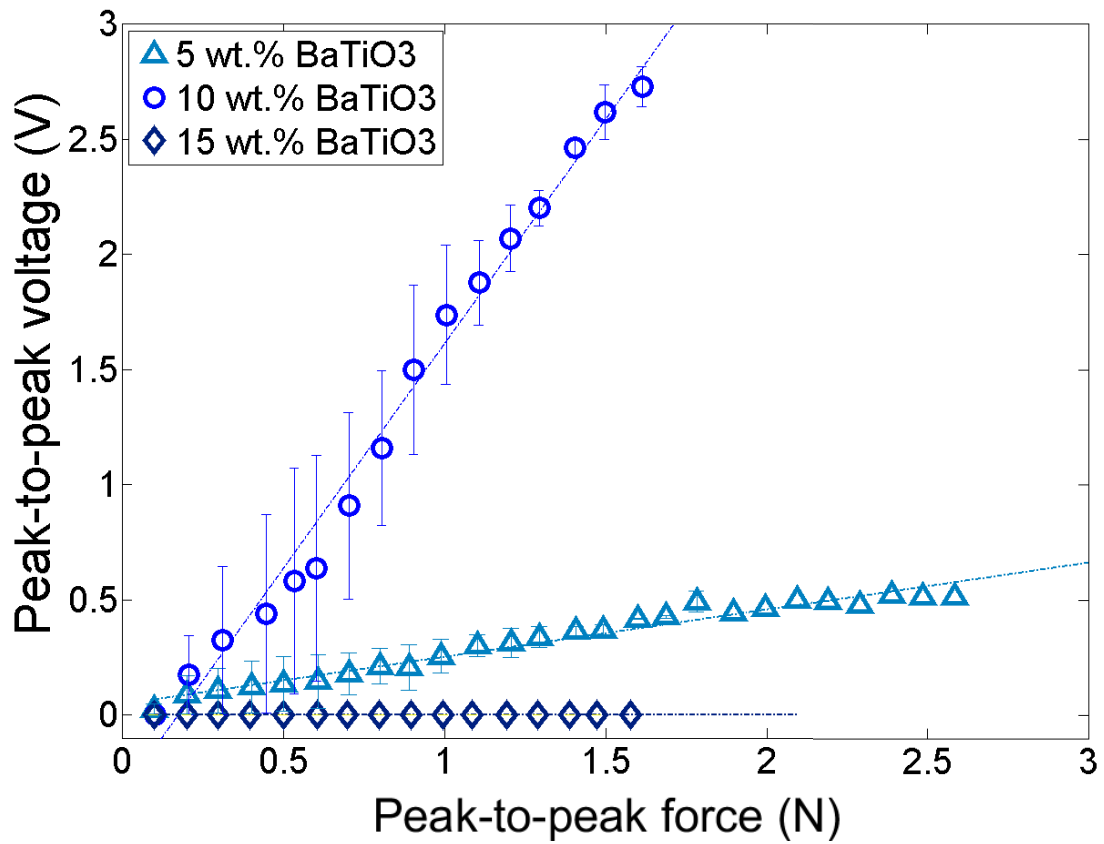


Figure 5. Peak-to-peak voltage as a function of peak-force at an excitation frequency of 45 Hz for 5, 10 and 15 wt.% of BaTiO₃ NP addition to PVDF via ball-milling.

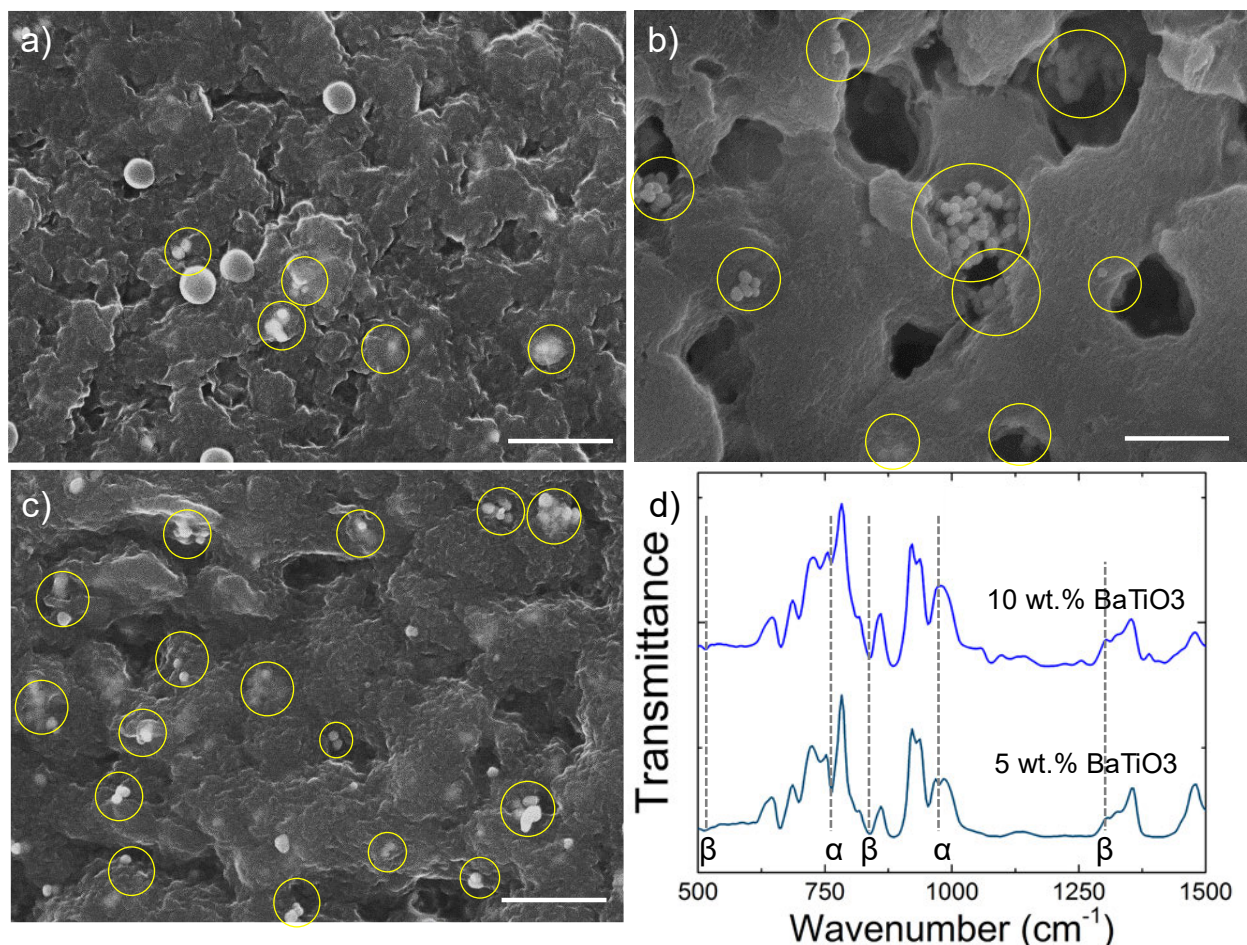


Figure 6: SEM image of surfaces of films fabricated from the 0.2 g mL^{-1} ball-milled nanocomposite solutions of (a) 5 wt.% BaTiO₃/ 95 wt.% PVDF; (b) 10 wt.% BaTiO₃/ 90 wt.% PVDF; (c) 15 wt.% BaTiO₃/ 85 wt.% PVDF (scale bar = 1 μm). Yellow circles highlight BaTiO₃ NP agglomerates; (d) FTIR curves of 5 wt.% BaTiO₃/ 95 wt.% PVDF and 10 wt.% BaTiO₃/ 90 wt.% PVDF (printing parameters: $\sim 1 \text{ MPa}$, 20 mm s^{-1} with a $100 \mu\text{m}$ nozzle).

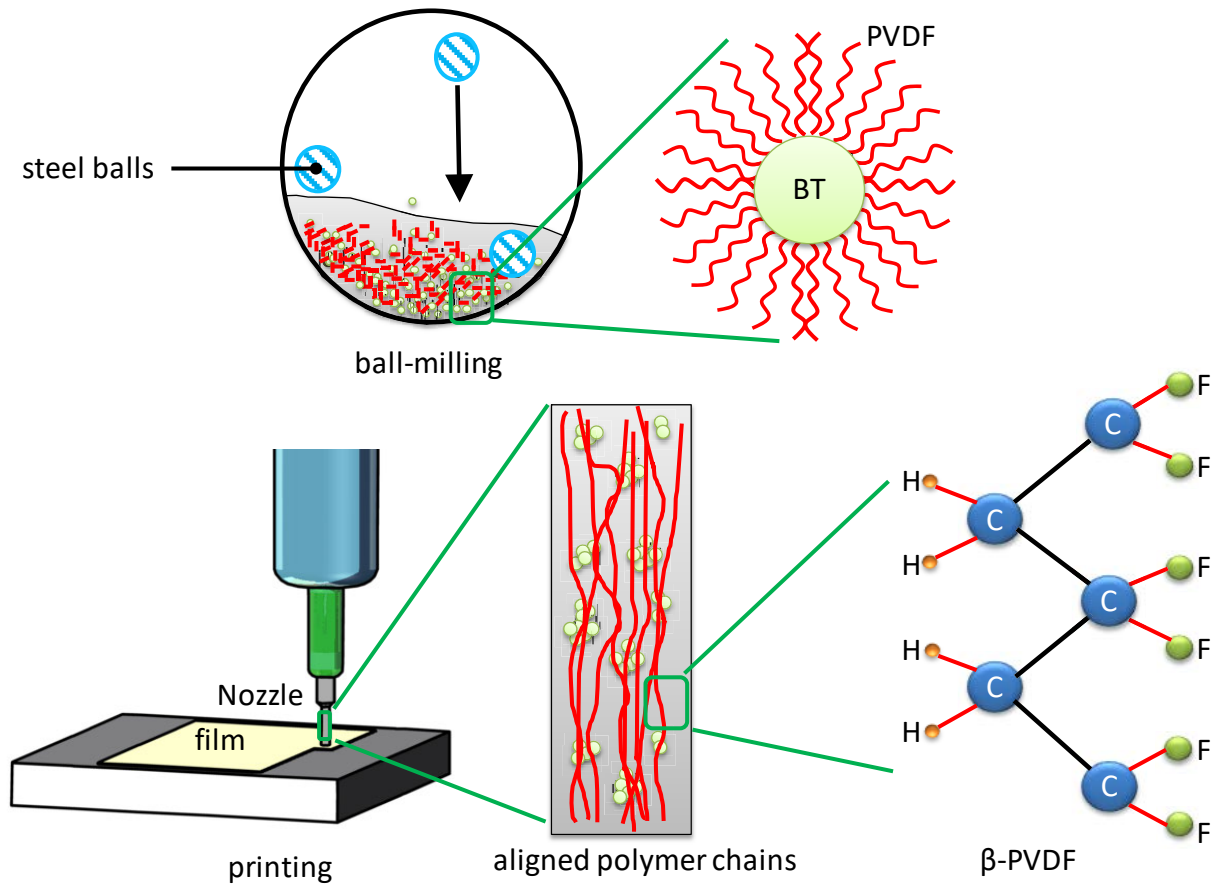


Figure 7. Schematic of the proposed process leading to increase in β -phase fraction in PVDF due to filler addition. Ball-mill mechanically activates the BaTiO₃ NPs (BT) which provides adhesion sites for PVDF chains. The polymer chains crystallize into aligned β -phase upon extrusion through the nozzle. The NP agglomerates arrest the PVDF chains in the β -phase upon solidification, thus leading to improved piezoelectric properties.

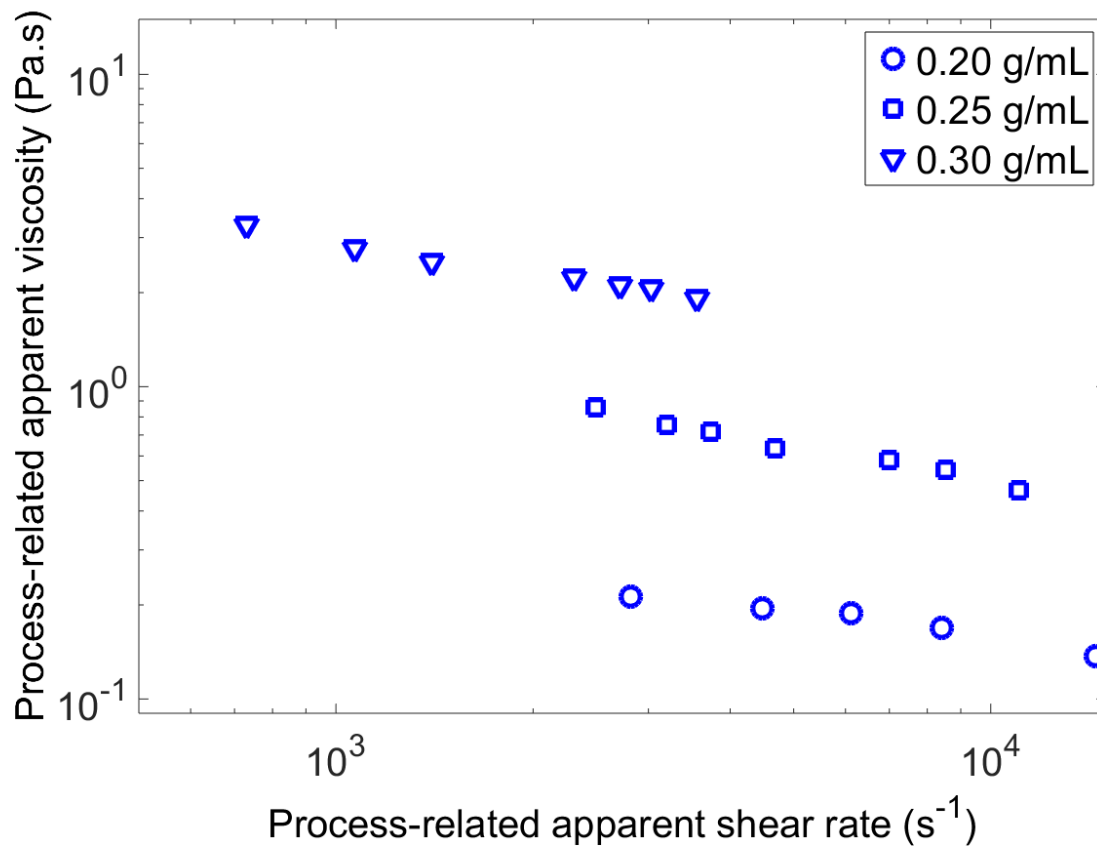


Figure 8. Viscosity as a function of shear rate during the printing process for 0.20, 0.25, and 0.30 g mL⁻¹ of the ball-milled nanocomposite with 10 wt.% BaTiO₃ NPs (printing parameters: 0.5 mm s⁻¹ with a 100 μm nozzle).

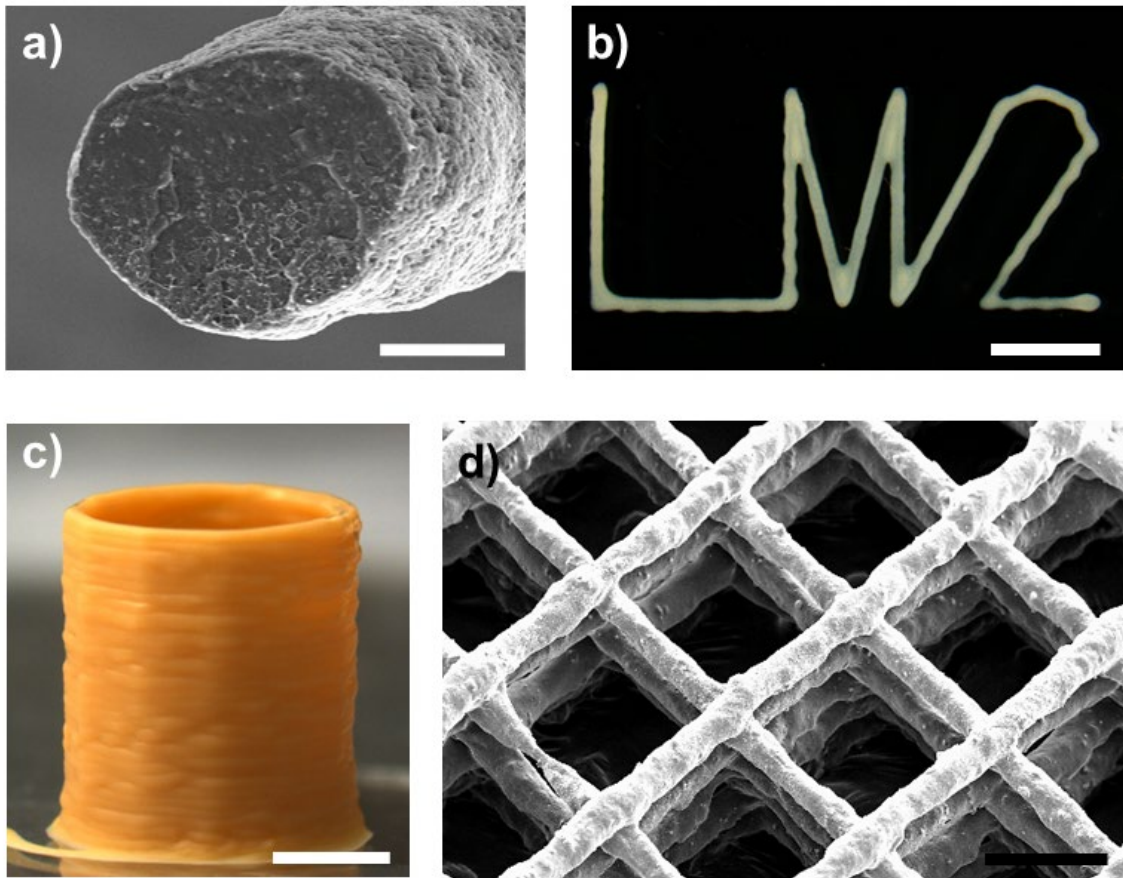


Figure 9. Structures fabricated using 10 wt.% BaTiO₃ ball-milled nanocomposite solution. (a) SEM image of cross-sectional view of a 1D fiber (scale bar = 25 μm); (b) optical microscopy image of a 2D structure reading ‘LM2’ (the abbreviation of the ‘Laboratory of Multiscale Mechanics’; scale bar = 2.5 mm); (c) photograph of inclined side-view of a 2.5D 70-layer circular cylinder (scale bar = 2 mm); (d) SEM image of inclined top-view of a 3D spanning 9-layer scaffold (scale bar = 0.5 mm).

ASSOCIATED CONTENT

Supporting Information. The Supporting Information is available free of charge via the Internet at <http://pubs.acs.org>” and DOI:

Quasi-static tests and Multi-frequency piezoelectric tests with DMA of PVDF nanocomposites, Additional information on piezoelectric coefficient calculations, SEM of the cross-sections of films fabricated from ball-milled, extruded and sonicated nanocomposites, XRD of the films prepared by ball-milling with different NP loadings in PVDF, Ferroelectric characterization, Apparent viscosity calculation, 3D printed sensor testing (PDF)

AUTHOR INFORMATION

Corresponding Author

*daniel.therriault@polymtl.ca

Author Contributions

The manuscript was written through the contributions of all authors. All authors have given approval to the final version of the manuscript.

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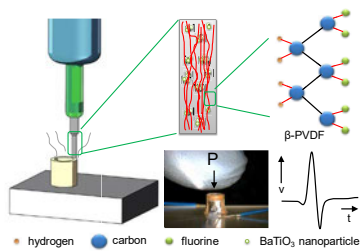
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Table of Contents Graphic



Supporting Information

ONE-STEP SOLVENT EVAPORATION-ASSISTED 3D PRINTING OF PIEZOELECTRIC
PVDF NANOCOMPOSITE STRUCTURES

*SAMPADA BODKHE, GABRIELLE TURCOT, FREDERICK P. GOSSELIN AND DANIEL
TERRIAULT**

AUTHOR ADDRESS

Laboratory for Multiscale Mechanics, Department of Mechanical Engineering,
Centre for Applied Research on Polymers and Composites (CREPEC)
Polytechnique Montreal,
C.P. 6079, succ. Centre-Ville, Montreal, QC H3C 3A7, Canada

Corresponding Author

*daniel.therriault@polymtl.ca

1. Mechanical tests with DMA

A dynamic mechanical analyser (DMA, Q800; TA instruments) was used in tension mode (Figure S1a) to investigate the maximum strain to be used for dynamic tests. Quasi static stress-strain tests with a controlled ramp force of 0.5 N min^{-1} were carried out on nanocomposite films (10 mm (grip separation) \times 5 mm \times 0.1-0.2 mm) prepared by the three mixing methods. Five samples were tested for each type of nanocomposite. The stress versus strain behaviour of each nanocomposite was determined to investigate the material stiffness and strength.

Figure S1b shows the averaged stress-strain curves for the three nanocomposites and neat PVDF films. Addition of fillers to PVDF resulted in decreased strength and strain at break. Nanocomposite samples prepared by both extrusion and sonication resulted in higher tensile strength as compared to ball-milled nanocomposites. The highest strength (8 MPa) and Young's modulus (110 MPa) was obtained for the sonicated films attributed to the well-dispersed nanoparticles. Extrusion-mixed nanocomposites possessed intermediate properties (strength \sim 6.4 MPa, modulus \sim 98 MPa). The ball-milled nanocomposites in turn exhibited significantly lower strength (even lower than that of PVDF) of 1.8 MPa with a low Young's modulus of 23 MPa. The porous nature of the ball-milled nanocomposites lead to lower effective Young's modulus¹. With a lower modulus, a material can have higher deformation for a specific stress and thus, allows the fabrication of sensors with lower structural influence on the sensed component they are placed upon, thereby increasing the strain transfer from the component to the sensor.

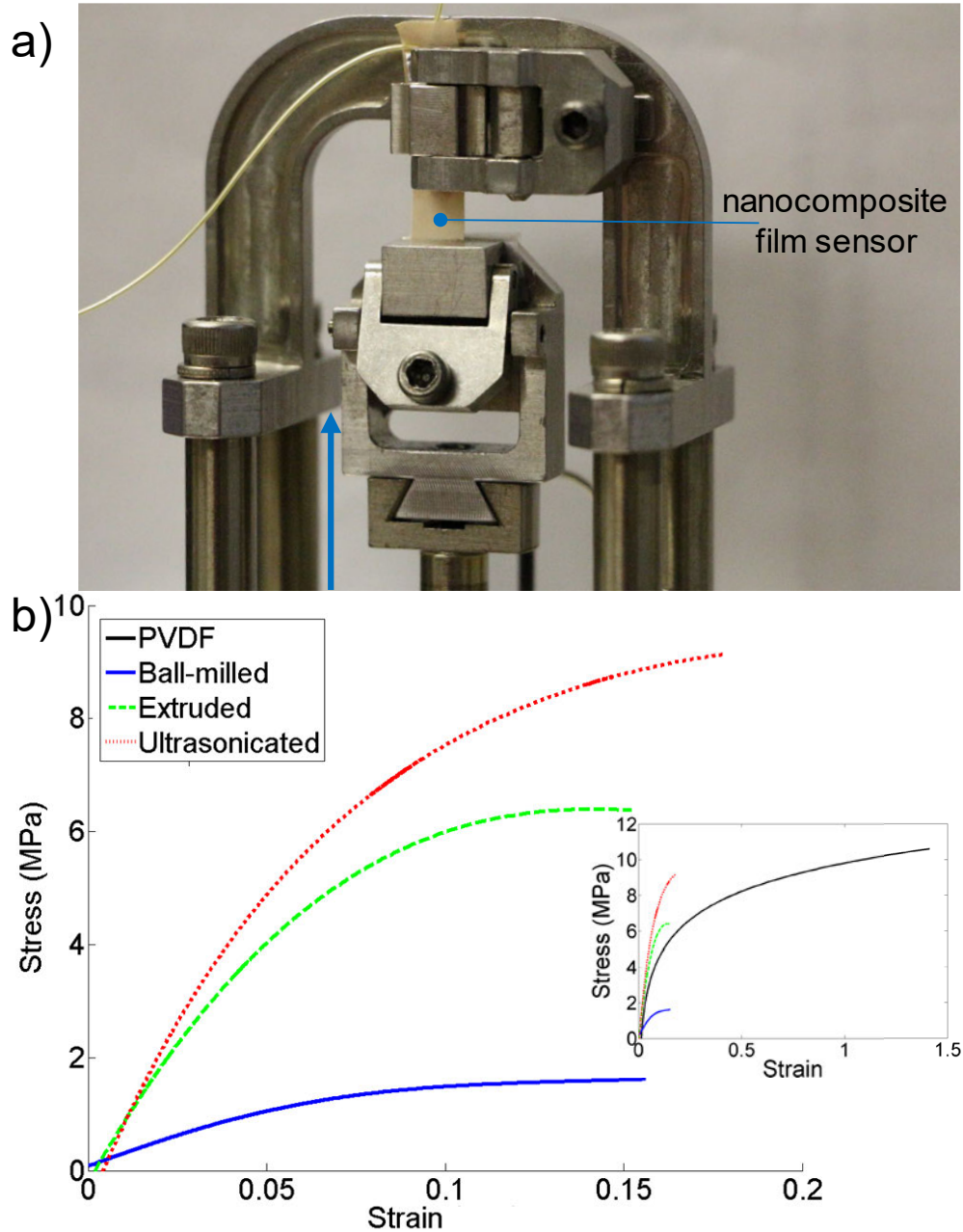


Figure S1: (a) Picture of the DMA used in tension mode with the nanocomposite test specimen. (b) Stress versus strain curves the nanocomposites prepared via ball-mill, extrusion and sonication mixing. The curve for PVDF can be seen in the inset.

2. Multi-frequency piezoelectric tests with DMA

A thin electrode layer (as shown in Figure S2) was painted on both sides of the printed films with commercially available conductive silver paste (Sigma Aldrich) to fabricate a sensor. The thickness of the painted silver electrode was about 15-20 μm and that of the nanocomposite films ranged from 150-200 μm as seen from the SEM image in Figure S2. Painting of silver instead of printing aided in achieving a comparatively thinner layer of silver (hence flexible) as the high viscosity of the silver paste limited its printability.

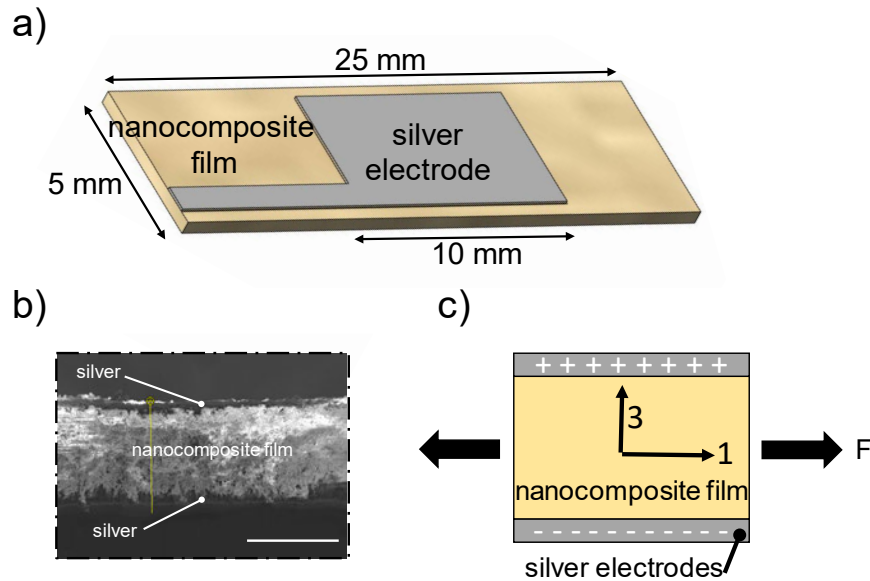


Figure S2: (a) Schematic of the sensor fabricated by painting silver electrode on the surfaces of the films. (b) SEM image of the cross-section of a representative nanocomposite sensor (scale bar = 200 μm). (c) Schematic of the phenomenon of charge generation in the sensor when subjected to forced excitation.

For the multi-frequency piezoelectric tests, the DMA was used in tension mode with a displacement amplitude of 50 μm (selected from the results of the quasi static tests). Tests were conducted on the films sensors (three samples for each processing technique with 10 wt.% filler loading) with average dimensions $6 \times 20 \times 0.1$ mm. Rectangular electrodes (10×5 mm) were

silver painted on each side of the sensors (see schematic Figure S3a). The scans were carried out from 1 to 80 Hz in 20 steps. Piezoelectric charges obtained from the sensors were converted into voltages using a charge amplifier (MEAS specialties) and acquired with a data acquisition system: NI-9239, attached to a USB carrier NI-9162 (National Instruments) and recorded using a LabVIEW interface. Figure S3a shows that the maximum voltage output was obtained with sensors fabricated from the ball-milled nanocomposites whereas films fabricated from the other two methods failed to give outputs distinguishable from the electrical noise. The response of the sensor, although linear with respect to the force, shows a gradual increase until a frequency of 35 Hz and then stabilizes around ~6 V as the force reaches a plateau. This mismatch in the early region of the voltage versus stress curve can be attributed to the internal dipole alignment in the sensors owing to the repeated stretching during the test.²⁻³ Additionally, to study whether the exhibited piezoelectricity was due to the PVDF or the NPs, nanocomposites were prepared by ball-milling 10 wt.% of NPs in polylactide (PLA) and dichloromethane (solvent for PLA). The fabrication process was similar to that used for the ball-milled PVDF nanocomposites. There was no voltage output in case of the PLA based nanocomposites; instigating the fact that the given process works because of the improved β -phase in PVDF and to attain the piezoelectric properties from the NPs, poling treatment would be a necessity.

A representative low frequency (for easier representation) voltage versus time output of the ball-milled sensors at 5 Hz is shown in Figure S3b. The curve resembles closely to the sinusoidal input of the DMA at 5 Hz.

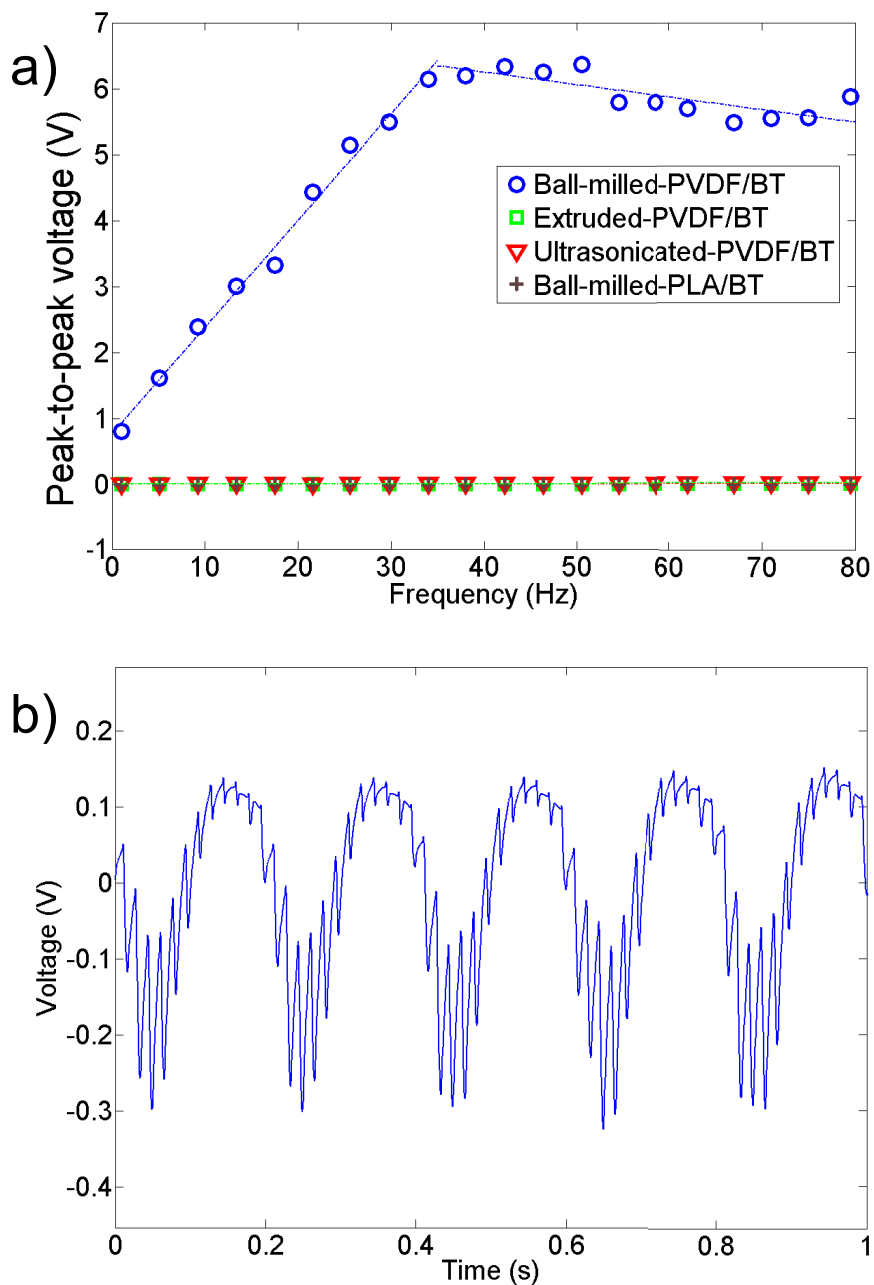


Figure S3. Peak-to-peak voltage output as a function of frequency for the three nanocomposite sensors with 10 wt.% BaTiO₃ NPs (BT) prepared by: ball-milling, extrusion and sonication and the PLA sensor (applied sinusoidal displacement from 0 to 50 μm). (b) Representative signal of sensor fabricated from the ball-milled nanocomposite with 10 wt.% BaTiO₃ nanoparticles at 5 Hz (filtered signal: Butterworth filter, band pass 1-10 Hz).

3. Additional information on piezoelectric coefficient calculations

The d_{31} coefficients were calculated using the IEEE standard on piezoelectricity⁴ from the curves in Figure 5. The simplified version of the constitutive equations in terms of d_{31} for in plane stretching, can be written as⁵:

$$V = \frac{Q}{C} = \frac{T_1 d_{31} t}{\epsilon_r} \quad (\text{S1})$$

where V is the potential difference at the output, T_1 is the applied stress in 1-direction, t is the thickness of the film and ϵ_r the dielectric constant of the film at the given frequency. Here, 3 is the thickness direction of the film (charge collection/ voltage measurement direction) and 1 is the direction of application of force.

4. Scanning electron microscopy

SEM images of the cross-sections of the films fabricated from the nanocomposite prepared by the three mixing methods are shown in Figure S4. Micro-pores can be observed in the films of the ball-milled nanocomposite while the pores in case of the other two kinds of nanocomposites are very small as compared to those in ball-milling.

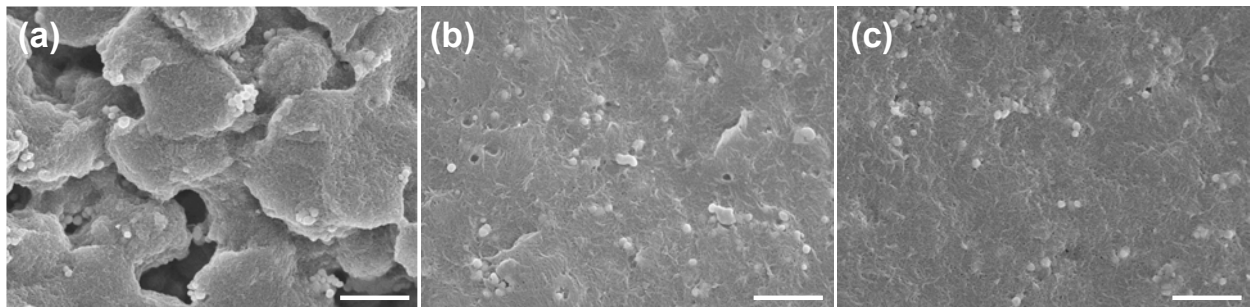


Figure S4. SEM images of fractured cross-sections of the films fabricated from the 0.2 g mL^{-1} nanocomposites (10 wt.% of BaTiO_3) in the solution prepared by (a) ball-milling; (b) extrusion and (c) sonication (scale bar = $1 \mu\text{m}$).

5. X-ray diffractometry

Figure S5 shows the diffractogram patterns of films printed from the nanocomposites prepared by ball-mill mixing of 5, 10 and 15 wt.% BaTiO₃ NPs with PVDF. Again, 10 wt.% BaTiO₃ nanocomposites crystallized completely in β -phase whereas the other two concentrations possessed peaks of α and γ -phases close to 18.7 and 40°, respectively. The decrease in piezoelectric properties further in case of 15 wt.% filler addition can also be a result of decrease in β -phase as well as the overall crystallinity of the nanocomposite at higher particle loadings.⁵⁻⁷ The degree of this decrease is again dependant on the particle shape and size, which is beyond the scope of this study.

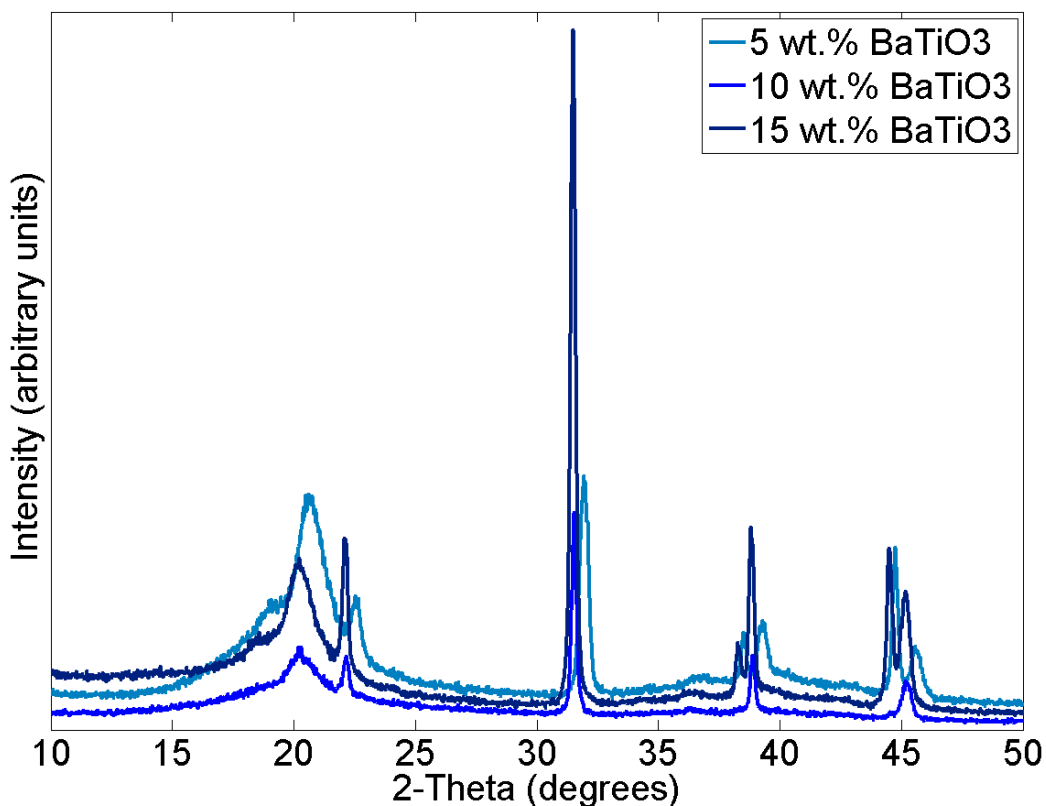


Figure S5: X-ray diffractogram of nanocomposite films prepared by ball-mill mixing with 5, 10 and 15 wt.% BaTiO₃ nanoparticles in PVDF.

6. Fourier Transform Infrared spectroscopy (FTIR)

The amount of β -phase amongst α and β -phases of PVDF is calculated with the help of Beer-Lambert law, which relates the absorption to the concentration of the species. The modified Beer-Lambert law for obtaining the fraction of β -phase is given by the equation below ⁸.

Fraction of β -phase,

$$F_{\beta} = \frac{A_{\beta}}{1.26A_{\alpha} + A_{\beta}} \quad (\text{S2})$$

where, A_{α} and A_{β} are the absorptions fractions of α and β -phases at 763 cm^{-1} and 840 cm^{-1} , respectively, and 1.26 is the ratio of absorption coefficients 7.7×10^4 and $6.1 \times 10^4 \text{ cm}^2\text{mol}^{-1}$ of β and α -phases, respectively.

7. Ferroelectric characterization of PVDF nanocomposites

Sensors for the impedance tests were separately fabricated by silver painting a circular area (diameter = 7 mm) on both sides of the nanocomposite films. Impedance tests to determine the dielectric constant and capacitance were performed using an impedance analyser (Agilent 4294A Precision) in the frequency range of 40 Hz to 1 kHz. The impedance values obtained from the tests were used to calculate the capacitance, C and the dielectric constant, ϵ_r , of the nanocomposites using the following formulae:^[9]

$$C = -\frac{1}{\omega} \left[\frac{Z_I}{Z_I^2 + Z_R^2} \right], \quad (\text{S3})$$

where Z_R and Z_I are real and imaginary parts of the impedance (Ω) and ω is frequency (rad s^{-1}).

The dielectric constant ϵ_r was evaluated from the definition of capacitance:

$$C = \varepsilon_0 \varepsilon_r \frac{A}{d}, \quad (\text{S4})$$

where ε_0 is the relative permittivity of free space ($8.854 \times 10^{-12} \text{ F m}^{-1}$), A is the area (m^2), and d (m) is the thickness of the sensor.

Table S1 and S2 show the variation of capacitance and dielectric constant values, respectively, for the nanocomposites prepared by three different approaches with the nanoparticle content at 45 Hz. Each value is an average of three samples.

Table S1: Variation of capacitance (pF) with nanoparticle loading in PVDF prepared by ball-milling, extrusion and sonication approaches at 45 Hz.

Sensor type	BaTiO ₃ content (wt.%)			
	0	5	10	15
PVDF	24			
Ball-milled		401	68	53
Extruded		379	77	140
Ultrasonicated		344	27	329

Table S2: Variation of dielectric constant with nanoparticle loading in PVDF prepared by ball-milling, extrusion and sonication approaches at 45 Hz.

Sensor type	BaTiO ₃ content (wt.%)			
	0	5	10	15
PVDF	9			
Ball-milled		171	210	76
Extruded		20	11	10
Ultrasonicated		16	36	88

Ferroelectric properties decreased for both the extrusion and ball-mill mixed nanocomposites after 10 wt.% particle addition. However, the ferroelectric properties continued to increase for the sonicated nanocomposite sensors. Ball-milled nanocomposites exhibited highest ferroelectric properties.

8. Process viscosity characterization of PVDF nanocomposites prepared by ball-milling:

To calculate the apparent viscosity of the solutions, shear stress τ_w was calculated from the applied pressures (neglecting the capillary flow effects as $L/D > 50$ ¹⁰) with the formula¹¹,

$$\tau_w = \Delta P \cdot \frac{D}{4L} \quad (S5)$$

where, ΔP is the difference between the applied pressure and atmospheric pressure.

The Newtonian shear rate is then given by

$$\gamma'_{Newt} = \frac{4Q}{\pi \left(\frac{D}{2}\right)^3} \quad (S6)$$

where, Q is the volumetric flow rate. To obtain the actual shear rate at the point of extrusion, we use Rabinowitch-Mooney correction parameter n defined by,

$$n = \frac{d \log(\tau_w)}{d \log(\gamma'_{Newt})} \quad (S7)$$

which is obtained from the slope of the log-log plot of shear stress versus Newtonian shear rate.

Then the shear rate is calculated by,

$$\gamma' = \gamma'_{Newt} \frac{3n+1}{4n} \quad (S8)$$

Finally, the apparent viscosity η_{app} is calculated as,

$$\eta_{app} = \frac{\tau_w}{\gamma'} \quad (S9)$$

9. 3D sensor testing

The 3D contact sensor was compared with a film sensor with the same electroded surface area as that of the cylindrical sensor. The test consisted of gently touching each sensor 3 times. The output voltages are presented in Figure S6. Where the film sensor generated a maximum voltage output of around -0.7 volts on touching (0.64 V on releasing), the 3D sensor produced up to 7.4 V (-1.7 V on releasing).

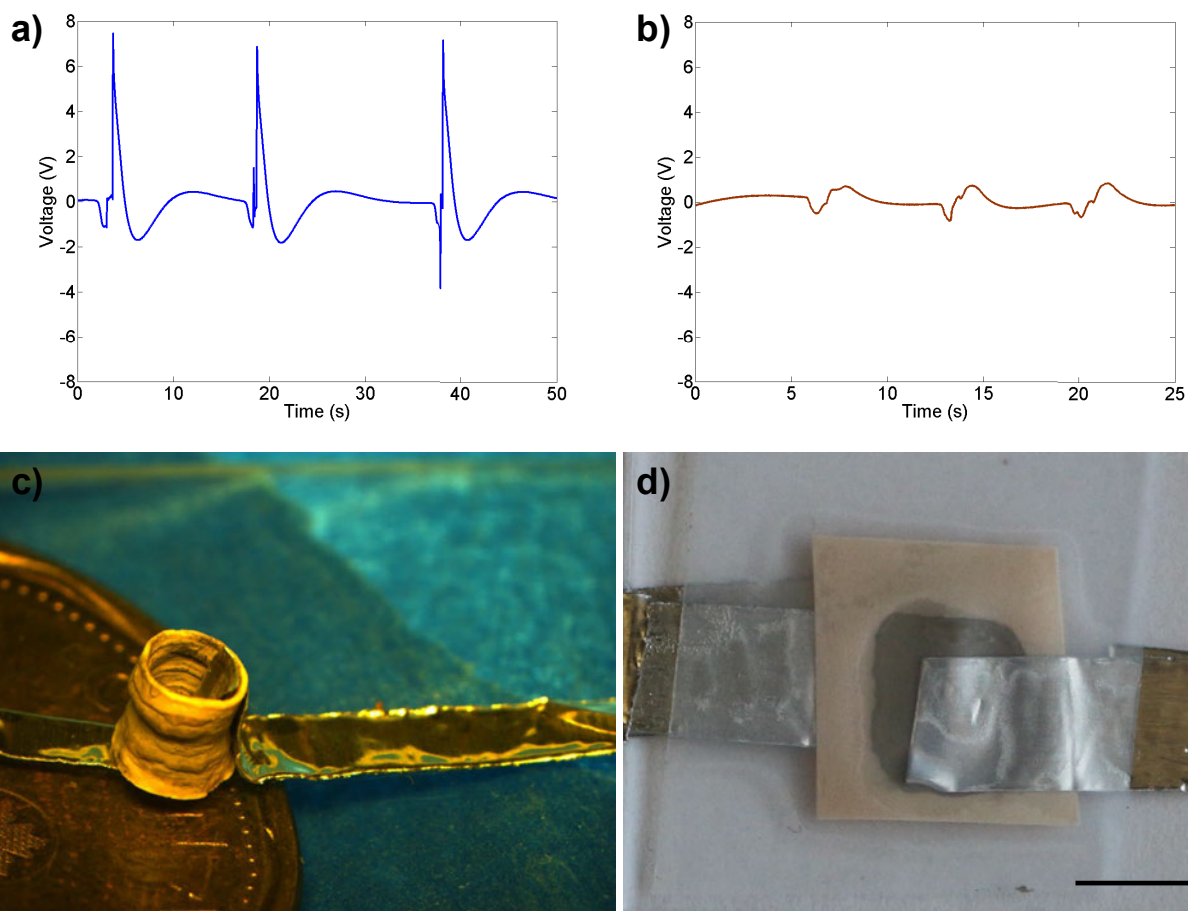


Figure S6: Sensor output voltages upon 3 consecutive taps: (a) 3D sensor; (b) film sensor. Pictures of the sensors (c) 3D sensor on a Canadian dollar coin and (d) film sensor (scale bar = 5 mm).

The following schematic (Figure S7) explains the working of the cylindrical sensor. As the cylindrical sensor is touched with a finger, the compression of the sensor creates a potential difference (depicted by the voltage peak in the positive direction). When the current starts flowing

across the circuit the voltage decreases as seen by the decaying signal.¹²⁻¹³ Once the finger is removed, the stress acting on the sensor is released causing the electron flow in the opposite direction. This is seen as the negative part of the signal. Due to the non-uniformity in the touch and release forces, the signal is asymmetric, similar to that found in the literature.^{12, 14-15} The frequency is the same as that of the touching. The voltage output generated by the sensor is a consequence of a combination of various piezoelectric modes as opposed to just the single mode in the case of film or fiber-based sensors.

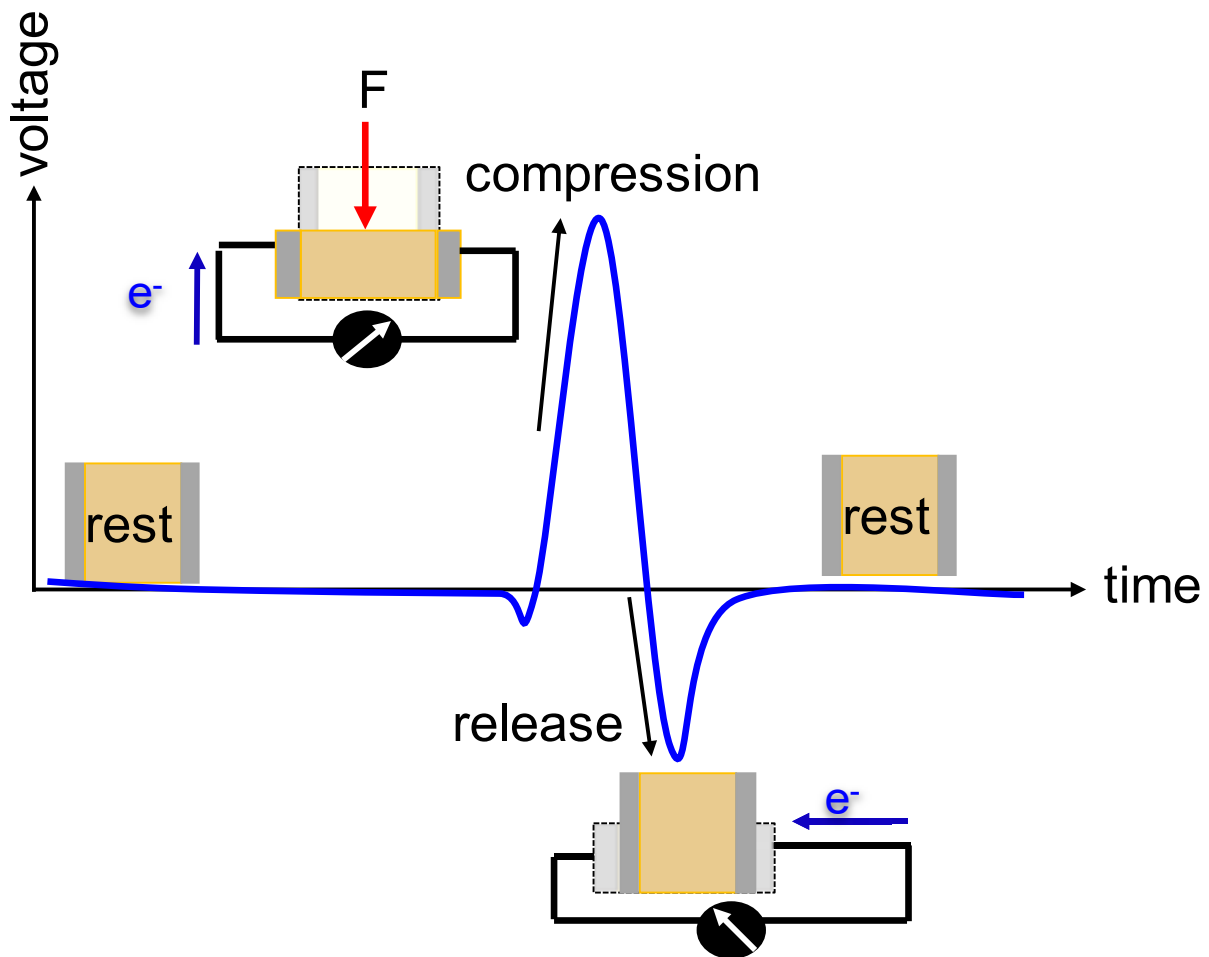


Figure S7: Schematic explaining the working of the sensor.

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